

# Maximal wall shear stress in carotid stenoses and of the circle of Willis

S.Lorthoais<sup>(1)</sup>, Cassot<sup>(2)</sup>, Maréchal<sup>(2)</sup> and Leger<sup>(3)</sup>

(1) Institut de Mécanique des Fluides de Toulouse, UMR CNRS 5502, 31400 Toulouse Cedex, France

(2) I.N.S.E.R.M. U 455, C.H.U. Purpan, 31059 Toulouse Cedex, France

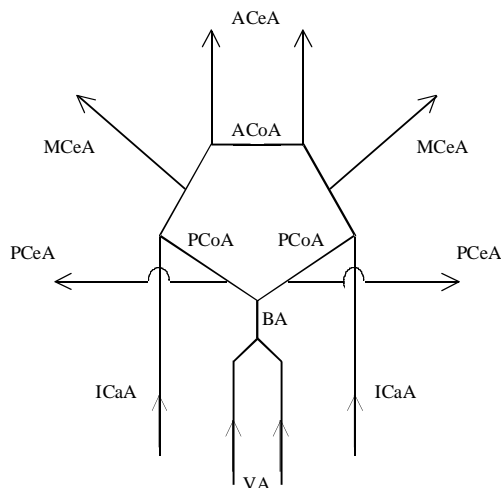
(3) Laboratoire de Modélisation en Mécanique, UMR CNRS 7607, 75252 Paris Cedex 5, France

## Background: Mechanisms of embolic material release

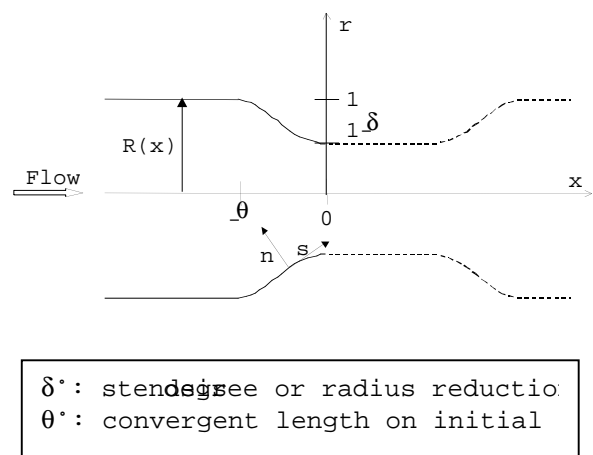
Elevated wall shear stresses encountered in advanced occlusive lesions of internal carotid arteries play an important role in the mechanism of atherosclerotic plaques rupture and thrombolytic combination with complex biological phenomena. In spite of an abundant literature about arterial stenoses, the importance of the underlying problem of circulation in the major cause of strokes which are themselves one of the most important cause of death and disability is little known. A few authors dealt with the evaluation of MWSS in stenoses, but none of them, the unique structure of cerebral macrocirculation, including an arterial network (loop), called the circle of Willis, and the afferent vessels - the internal carotid (ICA) and basilar (BA) arteries - and the efferent cerebral arteries -, was never taken into account in the assessment of this MWSS, though the flow rate through a carotid stenosis is highly dependent not only on its radius reduction but also on the collateral circulatory pathways of the circle of Willis [1]. In the present work, this factor on the MWSS in carotid stenoses is studied.

## Methods:

We computed the flow rate through a carotid stenosis as a function of the radius reduction and of the one on the opposite or contralateral side as well as of the diameter of a communicating (CoA) arteries. We used a non-linear one-dimensional unsteady mathematical model of flow through the circle of Willis [1, 2], considered as a network of twenty elastic vessels on Fig. 1.. The effects of the carotid stenoses were modeled by means of semi-empirical formulae of Young and Tsai [3] relating the pressure drop to the flow rate.



**Fig. 1. :** Diagram of the circle of Willis and its afferent and efferent arteries.



**Fig. 2. :** Geometry and nondimensional parameters of stenosis.

We calculated MWSS as a function of flow rate and geometry of stenosis, i.e., initial radius and radius reduction (Fig.2), by using the boundary layer theory and steady flow axisymmetry. After independence of MWSS on the entry velocity profile was demonstrated, the simple relationship between MWSS and the above parameters, which could be measured in clinical practice, was established.

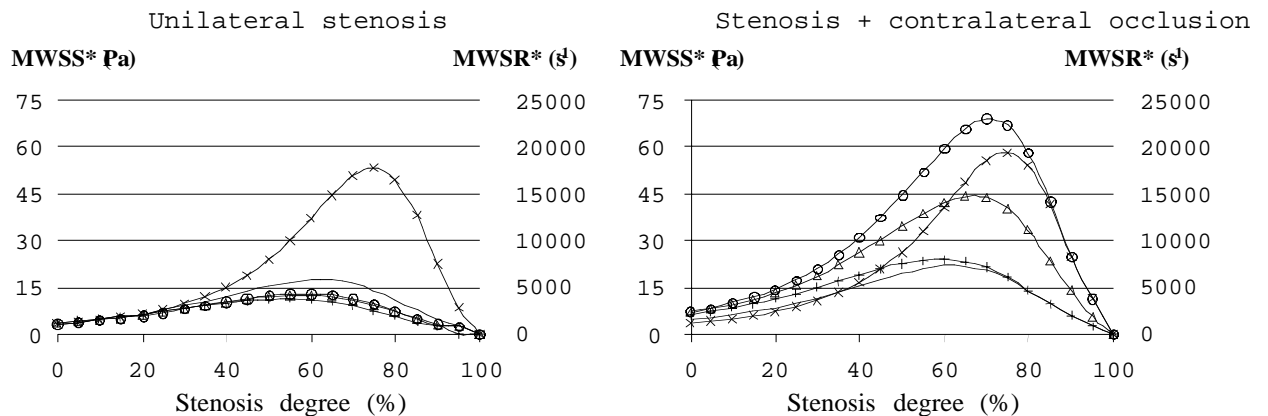
$$MWSS(\delta, Re_{eq}) = \frac{0,231}{(1-\delta)^{3,311}} \sqrt{Re_{eq}} + \frac{0,718}{(1-\delta)^{2,982}}, \quad Re_{eq} = \frac{Re_0}{\theta}$$

where  $Re_0$  is the Reynolds number based on the initial radius defined on Figure 2.

Note that such a relationship correlates accurately and extends the results found in resolution of Navier-Stokes equation for particular geometrical characteristics. Introducing in this formula the average flow rate computed by means of the network stenosed arteries can thus be analysed in the pathophysiological context of these lesions: their severity and the anatomy of the arterial network.

### Results: Huge variability of MWSS

Variations of MWSS as a function of stenosis degree (varying the stenotic degree by steps of different arrangements of anterior and posterior communicating arteries diameters (from ones to fully-functional large ones) emphasize the huge variability of this parameter (;



**Fig. 3.** : Dimensional maximal wall shear stress (MWSS\*) and rate (MWSR\*) as a function of stenosis degree, for five arrangements of anterior and posterior communicating arteries diameters ; x : ACoA=0.4 mm / PCoA=0.4 mm ; o : ACoA=0.4 mm / PCoA=1.6 mm ; o : ACoA=1.6 mm / PCoA=0.4 mm ; Δ : ACoA=1.6 mm / PCoA=1 mm ; + : ACoA=1.6 mm / PCoA=1.6 mm.

Whatever contralateral stenosis degree, MWSS is always maximal inside for stenosis between 60-80% - the value and position of this maximum depending on collateral circulatory path zero for occlusions.

For a given degree of unilateral stenosis (Fig 3, left), MWSS is maximal when collaterals are not efficient (both thin anterior and posterior communicating arteries).

For a given degree of stenosis associated to an occlusion (Fig. 3, right), MWSS is maximal when the anterior communicating artery is broad and the posterior communicating arteries are narrow. This results in a favourable collateral flow to the occluded side and an unfavourable increase in MWSS through the unilateral stenosis, leading to very high MWSS values (up to 55 Pa) in the stenosis (60%). This last result was obtained because we have not only considered an isolated stenosis but also included it in the whole network. It could explain the uncertainty about the percentage of carotid obstructive lesions that must be considered severe for the risk of stroke.

### Conclusion

Even so further investigations of the mechanical properties of thrombi and plaques are needed, understanding of the role of MWSS in the embolic mechanisms, our results suggest that the release could be maximum between 60 and 80% stenosis, where MWSS is maximal.

### References:

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